

Stress-Related Functional Connectivity Changes Between Auditory Cortex and Cingulate in Tinnitus

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Abstract

The question arises whether functional connectivity (FC) changes between the distress and tinnitus loudness network during resting state depends on the amount of distress tinnitus patients' experience. Fifty-five patients with constant chronic tinnitus were included in this study. Electroencephalography (EEG) recordings were performed and seed-based (at the auditory cortex) source localized FC (lagged phase synchronization) was computed for the different EEG frequency bands. Results initially demonstrate that the correlation between loudness and distress is nonlinear. Loudness correlates with beta3 and gamma band activity in the auditory cortices, and distress with alpha1 and beta3 changes in the subgenual, dorsal anterior, and posterior cingulate cortex. In comparison to non-tinnitus controls, seed-based FC differed between the left auditory cortices for the alpha1 and beta3 bands in a network encompassing the posterior cingulate cortex extending into the parahippocampal area, the anterior cingulate, and insula. Furthermore, distress changes the FC between the auditory cortex, encoding loudness, and different parts of the cingulate, encoding distress: the subgenual anterior, the dorsal anterior, and the posterior cingulate. These changes are specific for the alpha1 and beta3 frequency bands. These results fit with a recently proposed model that states that tinnitus is generated by multiple dynamically active separable but overlapping networks, each characterizing a specific aspect of the unified tinnitus percept, but adds to this concept that the interaction between these networks is a complex interplay of correlations and anti-correlations between areas involved in distress and loudness depending on the distress state of the tinnitus patient.

Key words: distress; seed-based connectivity; state dependent; tinnitus

Introduction

TINNITUS IS A SYMPTOM characterized by the perception of a sound in the absence of an external sound source. Most causes of tinnitus are related to transient or permanent deprivation of auditory input, associated to listening to loud music (Axelsson and Prasher, 2000), sudden sensorineural hearing loss (Schreiber et al., 2010), noise trauma (Folmer and Griest, 2003), or other causes. The development of tinnitus has been explained as a compensation mechanism to reduce deafferentation-related sensory uncertainty (i.e., lack of information) by filling in the missing auditory input (De Ridder et al., 2014a), which possibly explains its high prevalence in hearing loss (Axelsson and Ringdahl, 1989). Tinnitus can lead to or is associated with distress, an aversive state in which a patient with tinnitus is unable to adapt completely to stressors (i.e., tinnitus) resulting in distress and maladapt-

tive behaviors in about 20% of tinnitus patients (Axelsson and Ringdahl, 1989). This can lead to psychological complications such as annoyance, concentration problems, depression, anxiety, irritability, sleep disturbances, and intense worrying (Erlandsson and Holgers, 2001; Scott and Lindberg, 2000). Functional magnetic resonance imaging (fMRI) and magnetoencephalography (MEG) research has shown that tinnitus is often but not always (Langers et al., 2012) related to tonotopic map reorganization (Muhlnickel et al., 1998) and hyperactivity (Weisz et al., 2007) of the auditory cortex and that the subjectively perceived tinnitus loudness is correlated to increased gamma band activity in the auditory cortex as determined through electroencephalography (EEG) (van der Loo et al., 2009). The tinnitus-related distress, on the other hand, is related to activity in nonauditory brain systems (i.e., distress network), including the subgenual and dorsal anterior cingulate cortex, insula, as

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well as the posterior cingulate cortex as shown by structural and resting-state fMRI, EEG, and positron emission tomography (PET) research (De Ridder et al., 2011; Golm et al., 2013; Leaver et al., 2011; Schecklmann et al., 2013a; Vanneste et al., 2010a; Vanneste and De Ridder, 2012b).

Functional connectivity (FC) reflects temporal associations between separate brain areas and can be measured using lagged phase synchronization. Lagged phase synchronization can be interpreted as the amount of cross-talk synchronization between anatomically different brain regions (Congedo et al., 2010). FC is highly dynamic and stress dependent (van Marle et al., 2010). Tinnitus loudness can be associated with stress and negative mood (Dobie, 2003; Sullivan et al., 1988). Some theories of tinnitus pathophysiology even argue that negative emotional reactions to tinnitus are necessary for the disorder to become chronic (De Ridder et al., 2011; Jastreboff, 1990). If aversive reactions to tinnitus are necessary components of tinnitus pathophysiology, one might expect a relationship between the perceived loudness and amount of distress (De Ridder et al., 2011; Jastreboff, 1990). If tinnitus loudness is related to the amount of distress in tinnitus patients, it can be hypothesized that loudness related areas such as the auditory cortex (van der Loo et al., 2009) are functionally connected to the distress network (De Ridder et al., 2011; Golm et al., 2013; van der Loo et al., 2011; Vanneste et al., 2010a) in distressing tinnitus. A highly specific 10 and 11.5 Hz lagged phase synchronization has been shown between the parahippocampal area, and the subgenual anterior cingulate cortex in severely distressed patients (TQ grade 3 and 4 respectively) using EEG (Vanneste et al., 2014). However, recently, it has been suggested that the auditory cortex is also involved in tinnitus-related distress (Schecklmann et al., 2013b). How this auditory cortex involvement is governed is yet unknown.

In this article, we investigate whether the FC between the loudness and distress networks during resting-state EEG recordings is dependent on the amount of distress in tinnitus patients. Resting-state functional networks in the brain can be disentangled using lagged phase synchronization by applying seed-based FC. Seed-based FC allows mapping the resting state correlations of a single-seed region with every other voxel in the brain (Fox et al., 2006). We hypothesized that patients with distressing tinnitus show different FC patterns between the auditory cortex and the distress network system (De Ridder et al., 2011; Leaver et al., 2012; Maudoux et al., 2012a, 2012b; Vanneste et al., 2010a) depending on the amount of distress. As tinnitus loudness is related to gamma band activity in the auditory cortex, we take the auditory cortex as the seed for analyzing the FC differences related to the distress state.

Methods and Materials

Participants

Fifty-five patients ($M=48.31$ years; $SD=13.99$; 33 males and 22 females) with chronic constant tinnitus were included in this study. Tinnitus was considered chronic if its onset dated back 1 year or more. Individuals with pulsatile tinnitus, Ménière disease, otosclerosis, chronic headache, neurological disorders (i.e., brain tumors), and individuals being treated for mental disorders were excluded from the study to increase the sample homogeneity. This study was approved by the local

ethical committee (Antwerp University Hospital, Belgium) and was in accordance with the declaration of Helsinki.

All patients were interviewed as to their perceived location of the tinnitus (the left ear, in both ears, and centralized in the middle of the head [bilateral], the right ear) as well as for information related to the tinnitus sound (pure tone like tinnitus or noise-like tinnitus). In addition, all patients were screened for the extent of hearing loss using a pure tone audiometry according to the British Society of Audiology (2008) procedures at 0.125, 0.25, 0.5, 1, 2, 3, 4, 6, and 8 kHz. Tinnitus patients were tested for the tinnitus frequency through performance of a tinnitus matching procedure (Audiology, 2008). See Table 1 for an overview of the tinnitus characteristics.

Patients were also given the validated Dutch version of the Tinnitus Questionnaire (TQ) (Meeus et al., 2007) originally published by Goebel and Hiller (1994). Goebel and Hiller described the TQ as a global index of distress, and the Dutch version was further confirmed as a reliable measure for tinnitus-related distress (Meeus et al., 2007; Vanneste et al., 2011a). Based on the total score on the TQ, participants were assigned to a distress category: slight (0–30 points; grade 1), moderate (31–46; grade 2), severe (47–59; grade 3), and very severe (60–84; grade 4) distress (Goebel and Hiller, 1994; Meeus et al., 2007; Vanneste et al., 2011a). In addition, a numeric rating scale (NRS) for loudness (“How loud is your tinnitus?”: 0=no tinnitus and 10=as loud as imaginable’) was assessed.

Healthy control group

EEG data of a healthy control group ($N=55$; $M=48.33$ years; $SD=13.99$; 33 males and 22 females) was collected out of a large EEG database recorded with the same EEG equipment and matched for age and gender. None of these subjects was known to suffer from tinnitus. Exclusion criteria were known psychiatric or neurological illness, psychiatric history or drug/alcohol abuse, history of head injury (with loss of consciousness) or seizures, headache, or physical disability. For these healthy controls, hearing assessment was not performed.

EEG data collection

Recordings were obtained in a fully lighted room with each participant sitting upright on a small but comfortable chair. The actual recording lasted approximately 5 min.

TABLE 1. TINNITUS CHARACTERISTICS

Ear	
Left	14
Right	11
Bilateral	30
Tone	
Pure tone	25
Noise like	30
Tinnitus frequency (Hz)	
Arithmetic mean	5154.55 (SD=3144.47)
Hearing loss at the tinnitus frequency (dB HL)	
Arithmetic mean	28.24 (SD=15.11)
Hearing loss at the tinnitus frequency (dB SL)	
Arithmetic mean	6.69 (SD=8.93)

The EEG was sampled using Mitsar-201 amplifiers (Nova-Tech www.novatecheeg.com/) with 19 electrodes placed according to the standard 10–20 International placement (Fp1, Fp2, F7, F3, Fz, F4, F8, T7, C3, Cz, C4, T8, P7, P3, Pz, P4, P8, O1, O2) referenced to digitally linked ears analogous to what was done in the normative group. Impedances were checked to remain below 5 k Ω . Data were collected with the patients' eyes closed (sampling rate=500 Hz, band passed 0.15–200 Hz). Off-line data were, resampled to 128 Hz, re-referenced to average reference, band-pass filtered in the range 2–44 Hz, subsequently transposed into Eureka! software (Congedo, 2002), plotted, and carefully inspected for manual artifact-rejection. All episodic artifacts, including eye blinks, eye movements, teeth clenching, body movement, or ECG artifact, were removed from the stream of the EEG. Average Fourier cross-spectral matrices were computed for frequency bands delta (2–3.5 Hz), theta (4–7.5 Hz), alpha1 (8–10 Hz), alpha2 (10.5–12 Hz), beta1 (13–18 Hz), beta2 (18.5–21 Hz), beta3 (21.5–30 Hz), and gamma (30.5–44 Hz). These frequency bands are based on previous research with tinnitus (Vanneste et al., 2010b, 2011c; Vanneste and De Ridder, 2012a).

Source localization

Standardized low-resolution brain electromagnetic tomography was used (sLORETA; Pascual-Marqui, 2002). As a standard procedure, a common average reference transformation (Pascual-Marqui, 2002) is performed before applying the sLORETA algorithm. sLORETA computes electric neuronal activity as current density (A/m²) without assuming a predefined number of active sources. The solution space used in this study and associated lead field matrix are those implemented in the LORETA-Key software (freely available at www.uzh.ch/keyinst/loreta.htm). This software implements revisited realistic electrode coordinates (Jurcak et al., 2007) and the lead field produced by Fuchs and colleagues (2002) applying the boundary element method on the MNI-152 (Montreal neurological institute, Canada) template of Mazziotta and colleagues (2001). The sLORETA-key anatomical template divides and labels the neocortical (including hippocampus and anterior cingulate cortex) MNI-152 volume in 6,239 voxels of dimension 5 mm³, based on probabilities returned by the Demon Atlas (Lancaster et al., 2000). The coregistration makes use of the correct translation from the MNI-152 space into the Talairach and Tournoux space (Brett et al., 2002).

The tomography sLORETA has received considerable validation from studies combining LORETA with other more established localization methods such as fMRI (Mulert et al., 2004; Vitacco et al., 2002), structural MRI (Worrell et al., 2000), and PET (Dierks et al., 2000; Pizzagalli et al., 2004; Zumsteg et al., 2005). It was used in previous studies to detect activity in the auditory cortex (Vanneste et al., 2011b, 2011c; Zaehle et al., 2007). Further, sLORETA validation has been based on accepting as ground truth the localization findings obtained from invasive, implanted depth electrodes, in which case there are several studies in epilepsy (Zumsteg et al., 2006a, 2006c) and cognitive event-related potentials (Volpe et al., 2007). It is worth emphasizing that deep structures such as the anterior cingulate cortex (Pizzagalli et al., 2001) and mesial temporal lobes (Zumsteg et al., 2006b) can be correctly localized with these methods.

Seed-based phase synchronization

Phase synchronization between time series corresponding to different spatial locations are usually interpreted as indicators of the “functional connectivity.” Such “lagged phase coherence” between two sources can be interpreted as the amount of cross-talk between the regions contributing to the source activity (Congedo et al., 2010). Since the two brain areas oscillate coherently with a phase lag, the cross-talk can be interpreted as information sharing by axonal transmission. Any measure of dependence is highly contaminated with an instantaneous, nonphysiological contribution due to volume conduction (i.e., the transmission of electric or magnetic fields from an electric primary current source through biological tissue toward measurement sensors) (Pascual-Marqui, 2007b). However, Pascual-Marqui, (Pascual-Marqui, 2007a; Pascual-Marqui et al., 2011) introduced a new technique that removes this confounding factor. As such, this measure of dependence can be applied to any number of brain areas jointly, that is, distributed cortical networks, whose activity can be estimated with sLORETA. Measures of linear dependence (coherence) between the multivariate time series are defined. The measures are expressed as the sum of lagged dependence and instantaneous dependence. The measures are non-negative, take the value zero only when there is independence, and are defined in the frequency domain: delta (2–3.5 Hz), theta (4–7.5 Hz), alpha1 (8–10 Hz), alpha2 (10.5–12 Hz), beta1 (13–18 Hz), beta2 (18.5–21 Hz), beta3 (21.5–30 Hz), and gamma (30.5–45 Hz). Based on this principle, lagged linear connectivity was calculated. The auditory seeds were placed at the left and right auditory cortex (Table 2 for overview).

Regions of interest analyses

The log-transformed electrical current density was averaged across all voxels belonging to the regions of interest. Regions of interest were the left and right auditory cortex, the subgenual anterior cingulate cortex, the dorsal anterior cingulate cortex, and the posterior cingulate cortex. In addition, we opted for the seed-based FC to put the seed in the auditory cortex. These brain areas were predefined based on the MNI-coordinate, and based on the fact that they belonged to a specific Brodmann area on a standard brain. Regions of interest analyses were computed for the different frequency bands separately.

Statistics

Behavioral measures. To compare the TQ scores as well as the NRS for loudness for the different distress grades, we applied an ANOVA with as independent variable the grade (1, 2, 3, or 4) and as dependent variable, respectively, the TQ and the NRS for loudness. A simple contrast analysis

TABLE 2. SEEDS

	Seeds		
	<i>x</i>	<i>y</i>	<i>z</i>
Left auditory cortex	−46.1	−29.0	9.81
Right auditory cortex	46.7	−28.6	10.0

was used to compare the different grades from each other. This latter test includes a correction for multiple comparisons using a Bonferroni correction.

To verify the association between the loudness, as measured with the NRS, and the score on the TQ, we applied a Pearson linear correlation as well as a nonlinear (logarithmic) regression. For the comparison of variations between these two correlation outcomes (linear vs. nonlinear), we applied an *F*-test for equality of variances.

We applied a Chow test to determine whether the loudness has different impacts on different subgroups (i.e., distress grades) of the population. The Chow test is a statistical test evaluating whether the coefficients in two linear regressions on different data sets are equal and can be used to determine whether the variable (i.e., loudness) has a different impact on different subgroups (i.e., distress state) of the population. This Chow test follows an *F*-distribution. The Chow test was used to verify whether the association between loudness (NRS) and distress (TQ) was different between different tinnitus grades.

Functional measurements. A MANOVA was performed, including loudness (NRS) and distress (TQ) as independent variables and the log-transformed current density for different frequency bands, namely delta (2–3.5 Hz), theta (4–7.5 Hz), alpha1 (8–10 Hz), alpha2 (10.5–12 Hz), beta1 (13–18 Hz), beta2 (18.5–21 Hz), beta3 (21.5–30 Hz), and gamma (30.5–44 Hz), as dependent variables for the subgenual anterior cingulate cortex, the dorsal anterior cingulate cortex, the posterior cingulate cortex, and the auditory cortex. In addition, a logistic regression was used with TQ grade (low distress vs. high distress) as dependent variables and the different frequency bands, namely delta (2–3.5 Hz), theta (4–7.5 Hz), alpha1 (8–10 Hz), alpha2 (10.5–12 Hz), beta1 (13–18 Hz), beta2 (18.5–21 Hz), beta3 (21.5–30 Hz), and gamma (30.5–44 Hz) as independent variables for the posterior cingulate cortex.

To identify potential differences in brain electrical activity, voxel-by-voxel analysis using sLORETA was performed for each frequency band. Nonparametric statistical analyses of sLORETA images (statistical nonparametric mapping; SnPM) were performed for each contrast using sLORETA built-in voxelwise randomization tests (5000 permutations) and *t*-statistics for independent groups ($p < 0.05$). The SnPM methodology does not rely on any Gaussian assumptions by employing a locally pooled (smoothed) variance estimate that can outperform the Statistical Parametric Mapping approach (Segrave et al., 2011). SnPM's permutation method for correction for multiple comparisons (5000 permutations in the current study) has been proved similar to those obtained using a standard GLM approach with multiple comparisons corrections derived from random field theory (Holmes et al., 1996; Nichols and Holmes, 2002).

To determine differences in seed-based connectivity between the tinnitus groups and healthy controls, we performed *t*-statistics for independent groups with a corrected threshold $p < 0.05$, which were also corrected for multiple comparisons by conducting sLORETA-built-in voxelwise randomization tests (5000 permutations).

In addition, to correlate electrical brain activity, voxel by voxel, with distress as measured with TQ, and loudness as measured with NRS, a permutation test was used

that corrects for multiple comparisons by conducting sLORETA-built-in voxelwise randomization tests (5000 permutations).

Results

Behavioral measurements

Mean scores on distress and loudness. Table 3 shows the mean scores and standard deviations for distress as measured with the TQ (Goebel and Hiller, 1994; Meeus et al., 2007) and loudness as measured with an NRS. A significant difference was obtained for the distress when divided into distress states (i.e., grades), $F = 157.39$, $p < 0.001$. More importantly a significant effect was obtained for loudness when divided into distress states, $F = 5.55$, $p < 0.01$.

The relationship between loudness and distress. The linear correlation between NRS loudness and TQ revealed a significant positive correlation ($r = 0.47$, $p < 0.001$). In addition, a nonlinear correlation (logarithmic) between NRS loudness and TQ also revealed a significant positive correlation ($r = 0.51$, $p < 0.001$) (Fig. 1A). This nonlinear method explained 26% of the variance, whereas the linear method revealed 22% of the variance. An *F*-test between the difference of the R^2 's between two models in a single sample revealed a marginally significant effect ($F = 2.89$, $p = 0.09$).

We compared low distress (grade 1 and 2) tinnitus patients with high distress (grade 3 and 4) tinnitus patients and showed that a linear analysis of both groups separately is statistically relevant, $F = 3.03$, $p < 0.05$ using a Chow test. A linear correlation of two groups separately revealed a significant positive correlation for the patients with a low tinnitus-related distress ($r = 0.50$, $p < 0.001$) (Fig. 1B) and no significant correlation for grade 3 and 4 (Fig. 1E).

In addition, a Chow test was applied for the comparison between grade 1 and 2 tinnitus patients. This test revealed a significant effect, $F = 3.59$, $p < 0.05$. A linear correlation of two groups separately revealed a significant positive correlation for the patients with a low tinnitus-related distress ($r = 0.44$, $p < 0.001$) (Fig. 1C) and no significant correlation for grade 2 (Fig. 1D). Using a similar Chow test, it was also shown that a comparison between grade 1 and grade 3 and 4 tinnitus patients as well as a comparison between grade 2 and grade 3 and 4 tinnitus patients revealed a

TABLE 3. THE MEANS AND STANDARD DEVIATIONS OF TQ (DISTRESS) AND NRS (LOUDNESS) FOR THE TOTAL PATIENT GROUP AND PATIENTS WITH A GRADE 1, GRADE 2, GRADE 3, OR GRADE 4 SEPARATELY

		Grade				Total
		1	2	3	4	
Distress	M	20.72 ^a	38.23 ^b	52.00 ^c	72.75 ^d	40.53
	SD	7.65	5.50	3.57	5.60	18.70
Loudness	M	4.67 ^a	6.32 ^{a,b}	7.17 ^b	6.63 ^b	6.01
	SD	1.64	2.08	1.40	1.92	2.00
Patients		18	17	12	8	

Mean scores with a different superscript significantly differ from each other.

NRS, numeric rating scale; TQ, tinnitus questionnaire.

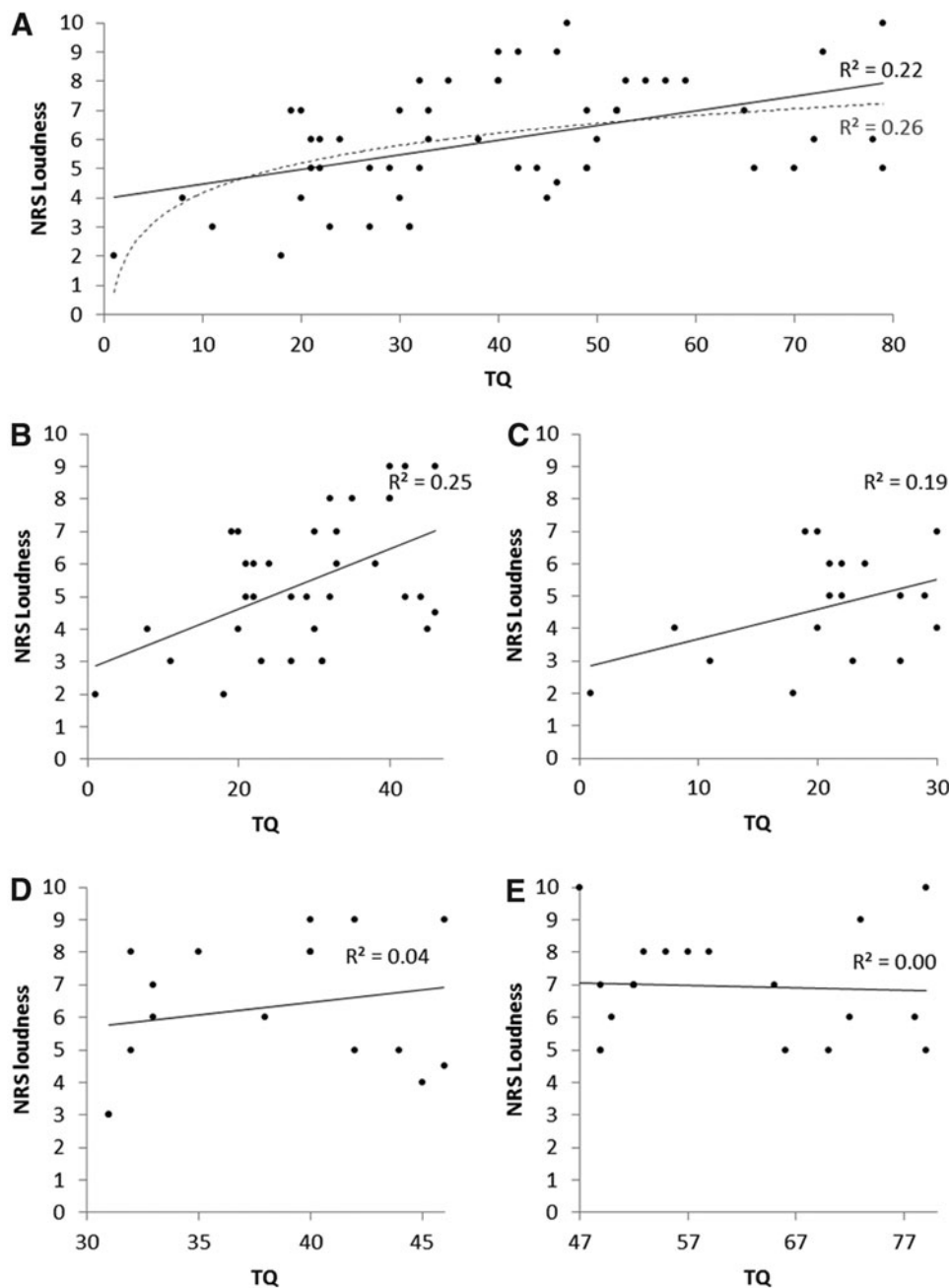


FIG. 1. Linear and nonlinear correlation between tinnitus-related distress as measured with the tinnitus questionnaire (TQ) and numeric rating scale (NRS) measuring loudness on the whole group of tinnitus patients (A); Correlation between distress and loudness for low distress (grade 1 and 2) tinnitus patients (B); Correlation between distress and loudness for very low distressed (grade 1) tinnitus patients (C); Correlation between distress and loudness for moderately distressed (grade 2) tinnitus patients (D); Correlation between distress and loudness for highly distressed (grade 3 and 4) tinnitus patients (E).

(marginally) significant effect, respectively $F=3.72, p<0.05$ and $F=2.70, p=0.06$.

Functional measurements

The relationship between specific brain areas and loudness and distress. Separate MANOVA's, including loudness (NRS) and distress (TQ) as independent variables and the log-transformed current density for different frequency bands as dependent variables for subgenual anterior cingulate cortex, the dorsal anterior cingulate cortex, the posterior cingulate cortex, and the secondary auditory cortex, were applied.

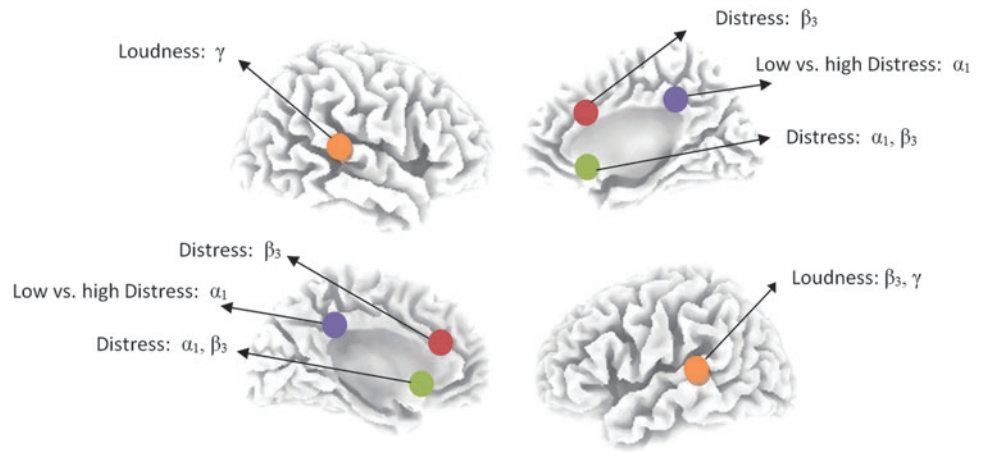
The subgenual anterior cingulate cortex revealed a significant effect for alpha1 ($F=4.08, p<0.05$) and beta 3 ($F=3.20, p<0.05$), but not for delta, theta, alpha 2, beta1,

beta2, and gamma ($p>0.17$). More specifically, between-subjects effects revealed for alpha1 ($F=6.72, p<0.01, \beta=14.31$) and beta3 ($F=6.43, p<0.02, \beta=10.52$) a significant effect for TQ, but not for loudness. Figure 2 gives an overview of the obtained results.

For the dorsal anterior cingulate cortex, the analysis revealed only a significant effect for beta3 (left: $F=3.58, p<0.05$ and right: $F=3.39, p<0.05$), but not for delta, theta, alpha1, alpha 2, beta1, beta2, and gamma ($p>0.26$). Between-subjects effects demonstrated that this was for TQ (left: $F=7.02, p<0.05, \beta=172.75$ and right: $F=6.82, p<0.05, \beta=167.70$), but not for loudness. See Figure 2 for overview.

For the posterior cingulate cortex, no significant effect was found. However, when applying a logistic regression with TQ grade (low distress vs. high distress) as dependent

FIG. 2. The significant effects of the log-transformed current density at the specific regions of interest (i.e., dorsal anterior cingulate cortex (red), subgenual anterior cingulate cortex (green), posterior cingulate cortex (purple), auditory cortex (yellow)) for the specific frequency bands on loudness and distress. Color images available online at www.liebertpub.com/brain



variables and the different frequency bands as independent variables, a significant effect ($\chi^2 = 15.79$, $p < 0.05$, Nagelkerke $R^2 = 0.40$) was revealed. A closer look at the data showed that this effect was obtained for, respectively, alpha 1 ($W = 5.74$, $p < 0.05$, $\beta = -2.56$) and alpha 2 ($W = 4.15$, $p < 0.05$, $\beta = -1.76$), demonstrating that the lower the log-transformed current density is in both frequency bands, the higher chance a patient has for high distress (grade 3 or 4) (Fig. 2). No significant effects were obtained for delta, theta, beta 1, beta 2, beta 3, and gamma.

For the left auditory cortex, a similar analysis was conducted that yielded a significant effect for beta 3 ($F = 5.25$, $p < 0.01$) and gamma ($F = 5.37$, $p < 0.01$), but not for delta, theta, alpha 1, alpha 2, beta 1, and beta 2 ($p > 0.12$). Between-subjects effects showed for beta 3 ($F = 5.25$, $p < 0.01$, $\beta = 3.67$) and gamma ($F = 10.49$, $p < 0.01$, $\beta = 11.91$) a significant effect for loudness, but not for TQ as indicated in Figure 2.

Similar analysis for the right auditory cortex revealed a significant effect for beta 3 ($F = 3.60$, $p < 0.05$) and gamma ($F = 5.64$, $p < 0.01$), but not for delta, theta, alpha 1, alpha 2, beta 1, and beta 2 ($p > 0.12$). Between-subjects effects showed for beta 3 ($F = 7.39$, $p < 0.01$, $\beta = 15.52$) and gamma ($F = 10.72$, $p < 0.01$, $\beta = 7.13$) a significant effect for loudness, but not for TQ. Figure 2 gives an overview of the obtained results.

Seed-based connectivity: Patients with tinnitus versus healthy control subjects. A comparison with the seed at the auditory cortex demonstrated increased lagged phase synchronization for the alpha 1 and beta 3 frequency bands for patients with tinnitus in comparison to healthy control subjects (Fig. 3). For the alpha 1 frequency, band-increased lagged phase synchronization was demonstrated with the posterior cingulate cortex (BA23) extending into the parahippocampal area. For the beta 3 frequency band, increased lagged phase synchronization was shown with the right insula (BA13), the posterior cingulate cortex (BA23), and the left (BA35) and right (BA28) parahippocampal area. No significant effect could be obtained in the delta, theta, alpha 2, beta 1, beta 2, and gamma frequency bands.

No significant results were obtained when placing the seed in, respectively, the right auditory cortex for delta, theta, alpha 1, alpha 2, beta 1, beta 2, beta 3, and gamma frequency bands.

The relationship between seed-based connectivity and distress. Seed-based lagged phase synchronization with the seed at, respectively, the left auditory cortex correlat-

ing with tinnitus-related distress as measured by the TQ revealed a significant effect for the alpha 1 and beta 3 frequency bands. For alpha 1 also, a decrease in lagged phase synchronization was found between the seed, the left secondary auditory cortex, and both the left inferior frontal gyrus (BA44) and the premotor cortex (BA6) in association with an increase in TQ (Fig. 4). For beta 3, it was shown that there was a

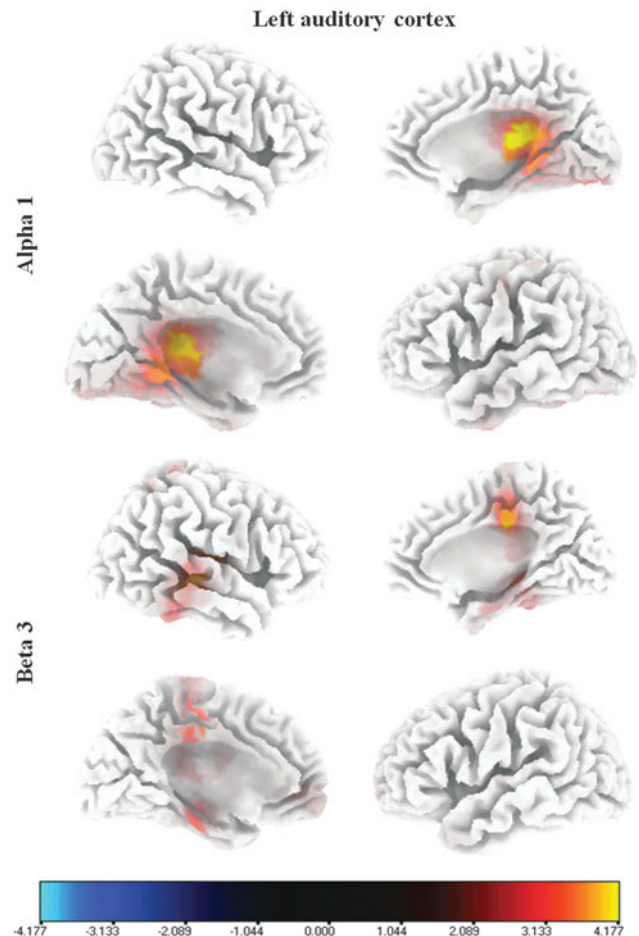


FIG. 3. A comparison between tinnitus patients and a healthy control group for the seed-based lagged phase synchronization with the seed at, respectively, the left auditory cortex. Color images available online at www.liebertpub.com/brain

decrease in lagged phase synchronization between the seed, respectively, in the left auditory cortex or secondary cortex auditory cortex and the dorsal anterior cingulate cortex (BA24) in association with an increase in TQ (Fig. 4). No significant results were obtained for delta, theta, alpha 2, beta1, beta2, and gamma frequency bands.

No significant results were obtained when placing the seed in, respectively, the right auditory cortex and correlating with tinnitus-related distress as measured with the TQ for delta, theta, alpha1, alpha 2, beta1, beta2, beta3, and gamma frequency bands.

The relationship between seed-based connectivity and loudness. Seed-based lagged phase synchronization with the seed at, respectively, the left auditory cortex, the right au-

ditory cortex correlating with tinnitus loudness revealed no significant effects for delta, theta, alpha1, alpha 2, beta1, beta2, beta3, and gamma frequency bands.

The relationship between seed-based connectivity and, respectively, grade 1, grade 2, and grade 3–4 tinnitus-related distress. Based on the finding that there is a difference in the relationship between the loudness and distress for, respectively, grade 1, grade 2, and grade 3–4, an analysis is performed to evaluate seed-based connectivity for, respectively, grade 1, grade 2, and grade 3–4 separately.

The relationship between seed-based connectivity and grade 1 tinnitus-related distress

When we apply seed-based lagged phase synchronization with the seed at the left auditory cortex, a significant effect could be obtained for the alpha2 frequency band, revealing an increased synchronization between the seed and the dorsal anterior cingulate cortex (BA24), but a decrease in the pregenual anterior cingulate cortex (BA32) in association with an increase on the TQ for grade 1 tinnitus patients (Fig. 5A). No significant effects could be demonstrated for delta, theta, alpha1, beta1, beta2, beta3, and gamma frequency bands.

No significant results were obtained when placing the seed in, respectively, the right auditory cortex and correlating with tinnitus-related distress for grade 1 tinnitus patients as measured with the TQ revealed for delta, theta, alpha1, alpha 2, beta1, beta2, beta3, and gamma frequency bands.

The relationship between seed-based connectivity and grade 2 tinnitus-related distress

Seed-based lagged phase synchronization with the seed at, respectively, the left auditory cortex, the right auditory cortex correlating with grade 2 tinnitus-related distress revealed no significant effects for delta, theta, alpha1, alpha 2, beta1, beta2, beta3, and gamma frequency bands.

The relationship between seed-based connectivity and grade 3 and 4 tinnitus-related distress

When we apply a similar analysis with the seed at the left auditory cortex, a significant effect could be obtained for the alpha2 frequency band, revealing an increased synchronization between the seed and the subgenual anterior cingulate cortex (BA25), in association with an increase on the TQ for grade 3 and 4 tinnitus patients (Fig. 5C). No significant effects could be demonstrated for delta, theta, alpha1, beta1, beta2, beta3, and gamma frequency bands.

No significant results were obtained when placing the seed in, respectively, the right auditory cortex and correlating with tinnitus-related distress for grade 3 and 4 patients for delta, theta, alpha1, alpha 2, beta1, beta2, beta3, and gamma frequency bands.

Discussion

The brain can be considered a highly dynamically complex adaptive system, adjusting its activity and FC constantly to accommodate for changes in the environment. Its primary aim is to reduce inherent uncertainty in the environment (De

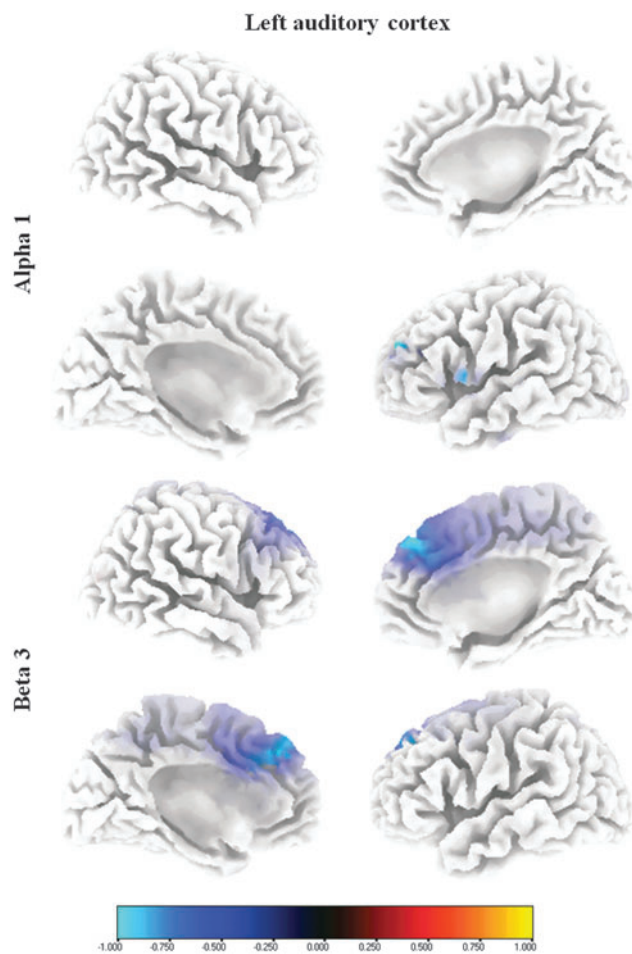
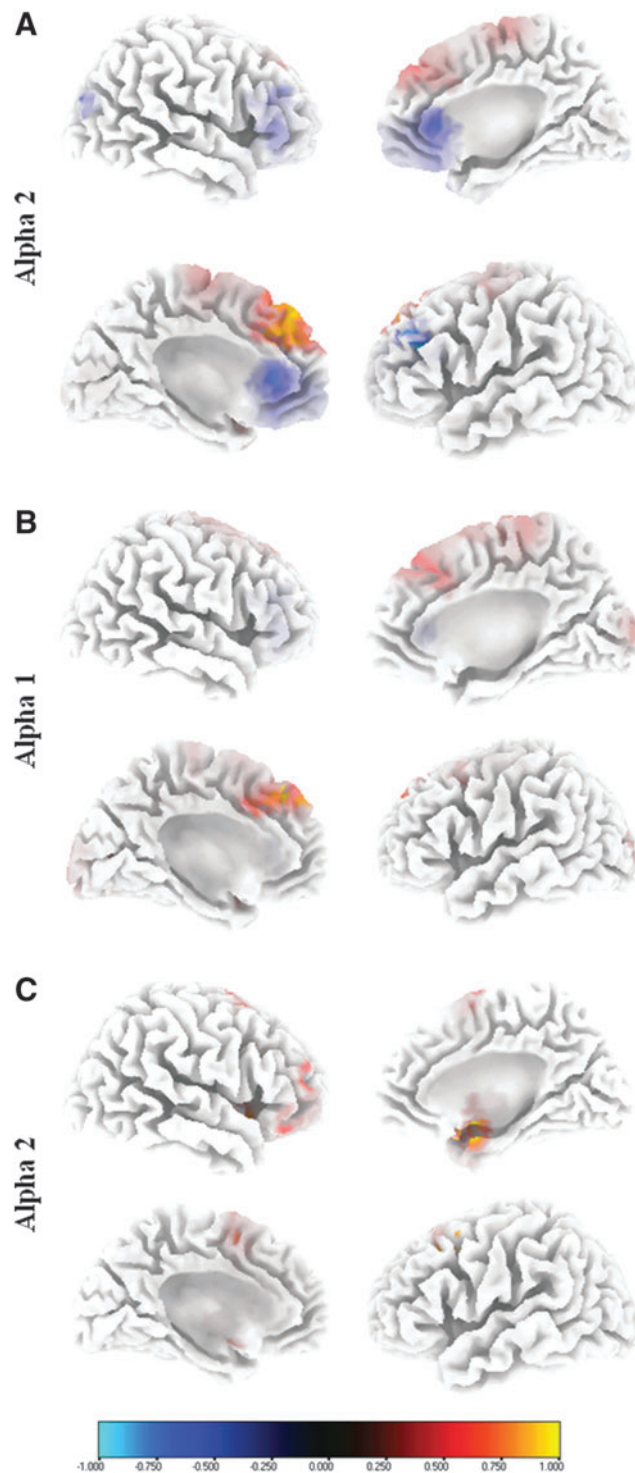


FIG. 4. Correlation for seed-based lagged phase synchronization with the seed at, respectively, left auditory cortex and distress as measured with the TQ. For alpha1 also, a decrease in lagged phase synchronization was found between the seed, the left secondary auditory cortex, and both the left inferior frontal gyrus (BA44) and the premotor cortex (BA6) in association with an increase in TQ. For beta3, it was shown that there was a decrease in lagged phase synchronization between the seed, respectively, in the left auditory cortex and the dorsal anterior cingulate cortex (BA24) in association with an increase in TQ. No significant results were obtained for delta, theta, alpha 2, beta1, beta2, and gamma frequency band. Color images available online at www.liebertpub.com/brain

Ridder et al., 2014a). Tinnitus can be regarded as a mechanism that resolves sensory uncertainty by filling in missing auditory information arising as a consequence of auditory deprivation (De Ridder et al., 2014a). In 1 out of 5 patients, this solution leads to or is associated with distress (Axelsson and Ringdahl, 1989; De Ridder et al., 2011). Distress is associated with changing FC between a loudness and distress network within the brain. The results provide new insights in how different brain networks interact in a complex way depending on the distress state of the tinnitus patient (see Figure 6).



The relationship between distress and loudness

Our data suggest that the subjectively perceived loudness (NRS) and distress (TQ) interact logarithmically, revealing a difference between the relationship of distress and loudness for, respectively, grade 1, 2, 3, and 4. That is, a strong relationship exists between loudness and distress for grade 1, while no significant relationship could be obtained for grades 2, 3, and 4. Based on these data, it can be hypothesized that patients with low distress can be stressed by variations of the loudness of the tinnitus; while in patients with higher distress, modulation of distress by loudness is very limited, that is, they are already distressed.

The frequency bands

Our main electrophysiological findings are related to the alpha and the beta frequency band. Using MEG, it has been demonstrated that long-range coupling between brain areas in “alpha and gamma networks” are related to tinnitus distress (Schlee et al., 2008) as are activity changes (Schlee et al., 2009; Weisz et al., 2005, 2007), whereas EEG studies have shown predominant changes in alpha and beta activity related to tinnitus distress (De Ridder et al., 2011; Vanneste et al., 2010a). Therefore, distress changes in FC are found in the same frequency bands as the activity changes.

The relationship between the distress and loudness dependent on the brain state

A correlation between the behavioral measure of distress and loudness revealed that a nonlinear correlation could better explain the results than a linear correlation ($r^2=0.26$ vs. 0.22). By splitting up the groups based on their distress state (respectively grade 1, 2, 3, and 4), a more detailed analysis revealed that there was a significant difference between loudness and distress between grade 1 and 2 distress states. Only grade 1 tinnitus patients, that is, those without distress, experience an increase in perceived loudness in correlation with increased distress or vice versa. It is of interest that this is not unique for tinnitus. When evaluating pain, which has pathophysiological (De Ridder et al., 2011), clinical (Moller, 1997, 2000, 2007), and treatment (De Ridder et al., 2007) analogies with tinnitus, a similar nonlinear

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FIG. 5. (A) Correlation for seed-based lagged phase synchronization with the seed at, respectively, left auditory cortex and distress as measured with the TQ. An increased synchronization between the seed and the dorsal anterior cingulate cortex (BA24), but a decrease in the pregenual anterior cingulate cortex (BA32) in association with an increase on the TQ for grade 1 tinnitus patients for alpha2 frequency band. (B) Correlation for seed-based lagged phase synchronization with the seed at, respectively, left auditory cortex and distress as measured with the TQ for grade 1 tinnitus patients. An increased synchronization between the seed and the dorsal anterior cingulate cortex (BA24); (C) Correlation for seed-based lagged phase synchronization with the seed at, respectively, left auditory cortex and distress as measured with the TQ for grade 3 and 4 tinnitus patients. Increased synchronization between the seed and the subgenual anterior cingulate cortex (BA25) was obtained. Color images available online at www.liebertpub.com/brain

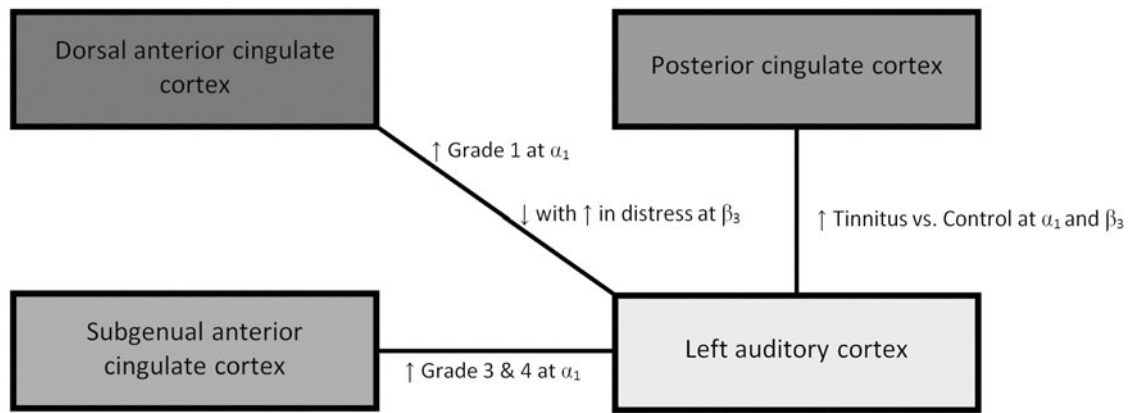


FIG. 6. An overview of the obtained results. Lower right box: brain area correlates with loudness at beta3 and gamma; lower left box: brain area correlates with distress at alpha1 and beta 3; upper left box: brain area correlates with distress at alpha1 and beta 3; upper right box: brain activity is different between low and high distress correlates of alpha1 and alpha2.

correlation is found between pain intensity and the affective components of pain (Litcher-Kelly et al., 2004). This could be related to the fact that scales are inherently nonlinear (Svensson, 2000), even though this seems not to be the case for low to moderate pain (Myles et al., 1999), or because the pain or tinnitus has to cross a threshold for it to become a salient stressor (Alpini and Cesarani, 2006; Hummel et al., 2010).

We confirm that subjectively perceived loudness is correlated with brain activity within the auditory cortex within the beta3 and gamma frequency band (van der Loo et al., 2009). These findings fit with the thalamocortical dysrhythmia that might underlie in tinnitus. The idea of Llinas and colleagues is that this abnormally persistent coupled theta-gamma band dysrhythmia is relayed to the cortex, selectively in the deaf-ferented thalamocortical columns (Llinás et al., 1999). Synchronized gamma band activity in the auditory cortex is proposed to bind auditory events into one coherent conscious auditory percept (Crone et al., 2001; Llinas et al., 1998; Ribary et al., 1991). It has been suggested that theta activity synchronizes large spatial domains (von Stein and Sarnthein, 2000) and binds together specific assemblies by the appropriate timing of spatially restricted higher-frequency localized oscillations (Buzsaki and Chrobak, 1995; Canolty et al., 2006; Engel et al., 2001; Varela et al., 2001) and that higher-frequency oscillations are confined to a small neuronal space, whereas very large networks are recruited by means of slow oscillations (Csicsvari et al., 2003; von Stein and Sarnthein, 2000). A recent study confirmed transient theta-gamma coupling and synchronizing geographically distributed gamma band activity in auditory attention (Doesburg et al., 2012). In tinnitus, it has been suggested that the normally waxing and waning theta gamma coupling remains permanently present (De Ridder et al., 2011) and intracranial recordings in a patient with simple auditory phantom. This disappears when tinnitus is suppressed by electrical stimulation of the auditory cortex (De Ridder et al., 2011).

However, when we correlated this loudness measurement with seed-based lagged phase synchronization with the seed at the auditory cortex, no FC differences were shown in contrast to the distress. Our data revealed that distress is positively correlated to activity in dorsal anterior cingulate cortex within the beta3 frequency band (De Ridder et al., 2011).

Brain state-dependent connectivity

For patients with tinnitus who have a relatively low amount of distress (i.e., grade 1), a strong correlation was shown between loudness and distress in the behavioral data. These findings are in accordance with the functional data. Grade 1 tinnitus patients demonstrated increased seed-based lagged phase synchronization between the auditory cortex seed and the dorsal anterior cingulate cortex in the alpha frequency band. Furthermore, there is decreased FC with the pregenual anterior cingulate cortex. This area is known to be involved in antinociception (Kong et al., 2010) as well as noise cancelling (De Ridder et al., 2012). This is in line with the hypothesis that dorsal anterior cingulate cortex is involved in persisting attention to the tinnitus but independent of loudness, as grade 1 tinnitus patients are usually only aware of the tinnitus when they are really focusing on the tone or noise, causing the loudness to increase due to a decreasing in the noise-cancelling mechanism (Leaver et al., 2011; Rauschecker et al., 2010). For grade 2 and grade 3–4 patients, there is no more change in loudness with increasing distress, possibly due to the fact that the FC has already decreased to zero, that is, no more modulation of the loudness is possible, in agreement with the clinical data. However, in grade 2 distress, the persisting FC between the auditory cortex and dorsal anterior cingulate cortex remains, suggesting too much attention is being paid to the tinnitus.

For tinnitus patients with a high distress (grade 3 and 4), increased alpha lagged phase synchronization is seen between the auditory seed and the subgenual anterior cingulate cortex associated with an increase in distress on the behavioral measurement. This goes together with this positive correlation between the distress on the behavioral measurement and the subgenual anterior cingulate cortex in both the alpha and the beta frequency band. Structural deficits have been observed in the subgenual cingulate cortex/nucleus accumbens (Leaver et al., 2011) and the subgenual anterior cingulate cortex. Alpha activity reflects the amount of tinnitus-related distress perceived by patients (Vanneste et al., 2010a). Previous research has demonstrated that subgenual cingulate cortex FC increases with increasing length of a depressive episode, suggesting that the resting-state

signal in the subgenual cingulate cortex region may be a marker for refractoriness to treatment (Greicius et al., 2007). In tinnitus, it has been shown that for grade 3 and 4 distress acts as a functional connection between the sgACC and the parahippocampal area exists at 10 Hz and 11.5 Hz, respectively, determining the amount of tinnitus-related distress. The sgACC is involved in autonomic control in tinnitus (Vanneste and De Ridder, 2013), mediated via theta activity. It is therefore possible that the alpha activity in high distress actually speeds up theta activity, analogous to the increasing speed seen in FC between the sgACC and parahippocampal area in increasing distress (Vanneste and De Ridder, 2013).

It is of interest that the anterior cingulate cortex is also involved in distress related to pain (Moisset and Bouhassira, 2007), somatoform disorders (Landgrebe et al., 2008), asthmatic dyspnea (von Leupoldt et al., 2009), and social rejection (Masten et al., 2009). As such, it is possible that when this non-specific distress network is already active and linked to the sound intensity encoding network (Schlee et al., 2008), it can result in the tinnitus sound being perceived as distressing.

The role of the auditory cortex

Although the right auditory cortex seems to be involved in the tinnitus loudness, these brain areas are not involved in the distress network. Confirmation for this hypothesis was further shown on the seed-based connectivity analyses, as there was no difference between healthy control subjects and tinnitus patients with the seed at, respectively, the right auditory cortex. An ongoing debate discusses whether tinnitus is always generated in the left or the contralateral auditory cortex (De Ridder, 2010). This debate arose because of dissimilar functional imaging results. Functional MRI (Melcher et al., 2000; Smits et al., 2007), MEG (Llinas et al., 2005; Muhlneckel et al., 1998; Weisz et al., 2007), and EEG (van der Loo et al., 2009) suggest the neural generator of the tinnitus is located in the contralateral auditory cortex, whereas most PET studies suggest tinnitus is always generated in the left auditory cortex (Arnold et al., 1996; Eichhammer et al., 2007). Other PET studies, however, report that left-sided auditory cortex activation is predominantly in left-sided tinnitus (Andersson et al., 2000) or irrespective of the tinnitus side (Arnold et al., 1996). Similar findings are demonstrated from modulating the auditory cortex. Several studies have demonstrated that using transcranial magnetic stimulation (TMS) targeting the left auditory cortex irrespective of the lateralization of tinnitus can suppress tinnitus (Kleinjung et al., 2008; Langguth et al., 2006). However, other studies using TMS or implanted extradural cortex stimulation reveal that modulating the contralateral auditory cortex to the tinnitus can also suppress tinnitus (De Ridder et al., 2007, 2010). Although our findings suggest that both the left and right auditory cortex are important in this respect, it is possible that, depending on the distress level, the left is more involved as it could indirectly influence distal areas connected to the auditory cortex. Previous research, indeed, already demonstrated that different neuromodulation techniques in general (Hallett, 2000; Kimbrell et al., 2002) or specific for tinnitus (Vanneste and De Ridder, 2011) influence distal brain areas functionally connected to the targeted area. Another possibility is that the right auditory cortex could be more involved in tinnitus-related

depression, as it has been shown that a similar network involving the parahippocampal area, sgACC, and orbitofrontal cortex is involved in both tinnitus-related distress and tinnitus-related depression but that these are lateralized, with distress lateralized to right parahippocampal area, right sgACC, and right orbitofrontal cortex and depression to the left homologue areas. Further research will have to verify this possibility.

Limitations

Due to the fact that sLORETA has a lower spatial resolution in comparison to fMRI and PET, we did not make a differentiation between the primary and secondary auditory cortex. This could be considered a potential weakness, as previous research has shown that there might be a difference between the primary and secondary auditory cortex.

Conclusion

These results suggest how the different brain areas interact in tinnitus is state dependent and related to the amount of distress the patients perceived. This corroborates with a recently proposed model that states that tinnitus is generated by multiple dynamically active separable but overlapping networks. Each network characterizes a specific aspect of the unified tinnitus percept (De Ridder et al., 2011, 2014b) but adds to this concept that the interaction between these networks is a complex interplay between specific brain areas involved in distress and loudness depending on the distress state of the tinnitus patient. This augments recent findings that during resting state, spontaneously distinct networks not only interact on the basis of their temporal nonstationary dependency (Smith et al., 2012) but also are dependent on the distress state in pathologies such as tinnitus.

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Author Disclosure Statement

No competing financial interests exist.

References

- Alpini D, Cesarani A. 2006. Tinnitus as an alarm bell: stress reaction tinnitus model. *ORL J Otorhinolaryngol Relat Spec* 68:31–36; discussion 36–37.
- Andersson G, Lyttkens L, Hirvela C, Furmark T, Tillfors M, Fredrikson M. 2000. Regional cerebral blood flow during tinnitus: a PET case study with lidocaine and auditory stimulation. *Acta Otolaryngol* 120:967–972.
- Arnold W, Bartenstein P, Oestreich E, Romer W, Schwaiger M. 1996. Focal metabolic activation in the predominant left auditory cortex in patients suffering from tinnitus: a PET study with [¹⁸F]deoxyglucose. *ORL J Otorhinolaryngol Relat Spec* 58:195–199.
- Audiology BSo. 2012. Recommended procedure: pure tone air and bone conduction threshold audiometry with and without masking and determination of uncomfortable loudness levels.

- www.thebsa.org.uk/wp-content/uploads/2014/04/BSA_RP_PTA_FINAL_24Sept11_MinorAmend06Feb12.pdf
- Axelsson A, Prasher D. 2000. Tinnitus induced by occupational and leisure noise. *Noise Health* 2:47–54.
- Axelsson A, Ringdahl A. 1989. Tinnitus—a study of its prevalence and characteristics. *Br J Audiol* 23:53–62.
- Brett M, Johnsrude IS, Owen AM. 2002. The problem of functional localization in the human brain. *Nat Rev Neurosci* 3:243–249.
- Buzsaki G, Chrobak JJ. 1995. Temporal structure in spatially organized neuronal ensembles: a role for interneuronal networks. *Curr Opin Neurobiol* 5:504–510.
- Canolty RT, Edwards E, Dalal SS, Soltani M, Nagarajan SS, Kirsch HE, Berger MS, Barbaro NM, Knight RT. 2006. High gamma power is phase-locked to theta oscillations in human neocortex. *Science* 313:1626–1628.
- Congedo M. 2002. *EureKa!* (Version 3.0) [Computer Software]. Knoxville, TN: NovaTech EEG, Inc. Freeware available at www.NovaTechEEG.
- Congedo M, John RE, De Ridder D, Prichep L, Isenhardt R. 2010. On the “dependence” of “independent” group EEG sources; an EEG study on two large databases. *Brain Topogr* 23:134–138.
- Crone NE, Boatman D, Gordon B, Hao L. 2001. Induced electrocorticographic gamma activity during auditory perception. *Brazier Award-winning article, 2001. Clin Neurophysiol* 112:565–582.
- Csicsvari J, Jamieson B, Wise KD, Buzsaki G. 2003. Mechanisms of gamma oscillations in the hippocampus of the behaving rat. *Neuron* 37:311–322.
- De Ridder D. 2010. Should rTMS for tinnitus be performed left-sided, ipsilaterally or contralaterally, and is it a treatment or merely investigational? *Eur J Neurol* 17:891–892.
- De Ridder D, De Mulder G, Menovsky T, Sunaert S, Kovacs S. 2007. Electrical stimulation of auditory and somatosensory cortices for treatment of tinnitus and pain. *Prog Brain Res* 166:377–388.
- De Ridder D, Elgoyhen AB, Romo R, Langguth B. 2011. Phantom percepts: tinnitus and pain as persisting aversive memory networks. *Proc Natl Acad Sci U S A* 108:8075–8080.
- De Ridder D, van der Loo E, Van der Kelen K, Menovsky T, van de Heyning P, Moller A. 2007. Theta, alpha and beta burst transcranial magnetic stimulation: brain modulation in tinnitus. *Int J Med Sci* 4:237–241.
- De Ridder D, van der Loo E, Vanneste S, Gais S, Plazier M, Kovacs S, Sunaert S, Menovsky T, van de Heyning P. 2011. Theta-gamma dysrhythmia and auditory phantom perception. *J Neurosurg* 114:912–921.
- De Ridder D, Vanneste S, Congedo M. 2011. The distressed brain: a group blind source separation analysis on tinnitus. *PLoS One* 6:e24273.
- De Ridder D, Vanneste S, Freeman W. 2014a. The Bayesian brain: Phantom percepts resolve sensory uncertainty. *Neurosci Biobehav Rev* 44:4–15.
- De Ridder D, Vanneste S, Menovsky T, Langguth B. 2012. Surgical brain modulation for tinnitus: the past, present and future. *J Neurosurg Sci* 56:323–340.
- De Ridder D, Vanneste S, van der Loo E, Plazier M, Menovsky T, van de Heyning P. 2010. Burst stimulation of the auditory cortex: a new form of neurostimulation for noise-like tinnitus suppression. *J Neurosurg* 112:1289–1294.
- De Ridder D, Vanneste S, Weisz N, Londero A, Schlee W, Elgoyhen AB, Langguth B. 2014b. An integrative model of auditory phantom perception: tinnitus as a unified percept of interacting separable subnetworks. *Neurosci Biobehav Rev* 44:16–32.
- Dierks T, Jelic V, Pascual-Marqui RD, Wahlund L, Julin P, Linden DE, ... Nordberg A. 2000. Spatial pattern of cerebral glucose metabolism (PET) correlates with localization of intracerebral EEG-generators in Alzheimer’s disease. *Clin Neurophysiol* 111:1817–1824.
- Dobie RA. 2003. Depression and tinnitus. *Otolaryngol Clin North Am* 36:383–388.
- Doesburg SM, Green JJ, McDonald JJ, Ward LM. 2012. Theta modulation of inter-regional gamma synchronization during auditory attention control. *Brain Res* 1431:77–85.
- Eichhammer P, Hajak G, Kleinjung T, Landgrebe M, Langguth B. 2007. Functional imaging of chronic tinnitus: the use of positron emission tomography. *Prog Brain Res* 166:83–88.
- Engel AK, Fries P, Singer W. 2001. Dynamic predictions: oscillations and synchrony in top-down processing. *Nat Rev Neurosci* 2:704–716.
- Erlandsson SI, Holgers KM. 2001. The impact of perceived tinnitus severity on health-related quality of life with aspects of gender. *Noise Health* 3:39–51.
- Folmer RL, Griest SE. 2003. Chronic tinnitus resulting from head or neck injuries. *Laryngoscope* 113:821–827.
- Fox MD, Snyder AZ, Zacks JM, Raichle ME. 2006. Coherent spontaneous activity accounts for trial-to-trial variability in human evoked brain responses. *Nat Neurosci* 9:23–25.
- Fuchs M, Kastner J, Wagner M, Hawes S, Ebersole JS. 2002. A standardized boundary element method volume conductor model. *Clin Neurophysiol* 113:702–712.
- Greicius MD, Flores BH, Menon V, Glover GH, Solvason HB, Kenna H, Reiss AL, Schatzberg AF. 2007. Resting-state functional connectivity in major depression: abnormally increased contributions from subgenual cingulate cortex and thalamus. *Biol Psychiatry* 62:429–437.
- Goebel G, Hiller W. 1994. [The tinnitus questionnaire. A standard instrument for grading the degree of tinnitus. Results of a multicenter study with the tinnitus questionnaire]. *HNO* 42:166–172.
- Golm D, Schmidt-Samoa C, Dechent P, Kroner-Herwig B. 2013. Neural correlates of tinnitus related distress: an fMRI-study. *Hear Res* 295:87–99.
- Hallett M. 2000. Transcranial magnetic stimulation and the human brain. *Nature* 406:147–150.
- Holmes AP, Blair RC, Watson JD, Ford I. 1996. Nonparametric analysis of statistic images from functional mapping experiments. *J Cereb Blood Flow Metab* 16:7–22.
- Hummel M, Cummons T, Lu P, Mark L, Harrison JE, Kennedy JD, Whiteside GT. 2010. Pain is a salient “stressor” that is mediated by corticotropin-releasing factor-1 receptors. *Neuropharmacology* 59:160–166.
- Jastreboff PJ. 1990. Phantom auditory perception (tinnitus): mechanisms of generation and perception. *Neurosci Res* 8:221–254.
- Jurcak V, Tsuzuki D, Dan I. 2007. 10/20, 10/10, and 10/5 systems revisited: their validity as relative head-surface-based positioning systems. *Neuroimage* 34:1600–1611.
- Kimbrell TA, Dunn RT, George MS, Danielson AL, Willis MW, Repella JD, ... Wassermann EM. 2002. Left prefrontal-repetitive transcranial magnetic stimulation (rTMS) and regional cerebral glucose metabolism in normal volunteers. *Psychiatry Res* 115:101–113.
- Kleinjung T, Vielsmeier V, Landgrebe M, Hajak G, Langguth B. 2008. Transcranial magnetic stimulation: a new diagnostic and therapeutic tool for tinnitus patients. *Int Tinnitus J* 14:112–118.
- Kong J, Loggia ML, Zyloney C, Tu P, Laviolette P, Gollub RL. 2010. Exploring the brain in pain: activations, deactivations and their relation. *Pain* 148:257–267.

- Lancaster JL, Woldorff MG, Parsons LM, Liotti M, Freitas CS, Rainey L, Kochunov PV, Nickerson D, Mikiten SA, Fox PT. 2000. Automated Talairach atlas labels for functional brain mapping. *Hum Brain Mapp* 10:120–131.
- Landgrebe M, Barta W, Rosengarth K, Frick U, Hauser S, Langguth B, Rutschmann R, Greenlee MW, Hajak G, Eichhammer P. 2008. Neuronal correlates of symptom formation in functional somatic syndromes: a fMRI study. *Neuroimage* 41:1336–1344.
- Langers DR, de Kleine E, van Dijk P. 2012. Tinnitus does not require macroscopic tonotopic map reorganization. *Front Syst Neurosci* 6:2.
- Langguth B, Zowe M, Landgrebe M, Sand P, Kleinjung T, Binder H, ... Eichhammer P. 2006. Transcranial magnetic stimulation for the treatment of tinnitus: a new coil positioning method and first results. *Brain Topogr* 18:241–247.
- Leaver AM, Renier L, Chevillet MA, Morgan S, Kim HJ, Rauschecker JP. 2011. Dysregulation of limbic and auditory networks in tinnitus. *Neuron* 69:33–43.
- Leaver AM, Seydell-Greenwald A, Turesky TK, Morgan S, Kim HJ, Rauschecker JP. 2012. Cortico-limbic morphology separates tinnitus from tinnitus distress. *Front Syst Neurosci* 6:21.
- Litcher-Kelly L, Stone AA, Broderick JE, Schwartz JE. 2004. Associations among pain intensity, sensory characteristics, affective qualities, and activity limitations in patients with chronic pain: a momentary, within-person perspective. *J Pain* 5:433–439.
- Llinas R, Ribary U, Contreras D, Pedroarena C. 1998. The neuronal basis for consciousness. *Philos Trans R Soc Lond B Biol Sci* 353:1841–1849.
- Llinas R, Urbano FJ, Leznik E, Ramirez RR, van Marle HJ. 2005. Rhythmic and dysrhythmic thalamocortical dynamics: GABA systems and the edge effect. *Trends Neurosci* 28:325–333.
- Llinás RR, Ribary U, Jeanmonod D, Kronberg E, Mitra PP. 1999. Thalamocortical dysrhythmia: A neurological and neuropsychiatric syndrome characterized by magnetoencephalography. *Proc Natl Acad Sci USA* 96:15222–15227.
- Masten CL, Eisenberger NI, Borofsky LA, Pfeifer JH, McNealy K, Mazziotta JC, Dapretto M. 2009. Neural correlates of social exclusion during adolescence: understanding the distress of peer rejection. *Soc Cogn Affect Neurosci* 4:143–157.
- Maudoux A, Lefebvre P, Cabay JE, Demertzi A, Vanhauzenhuyse A, Laureys S, Soddu A. (2012a). Auditory resting-state network connectivity in tinnitus: a functional MRI study. *PLoS One* 7:e36222.
- Maudoux A, Lefebvre P, Cabay JE, Demertzi A, Vanhauzenhuyse A, Laureys S, Soddu A. (2012b). Connectivity graph analysis of the auditory resting state network in tinnitus. *Brain Res* 1485:10–12.
- Mazziotta J, Toga A, Evans A, Fox P, Lancaster J, Zilles K, Woods R, et al. 2001. A probabilistic atlas and reference system for the human brain: International Consortium for Brain Mapping (ICBM). *Philos Trans R Soc Lond B Biol Sci* 356:1293–1322.
- Meess O, Blaivie C, Van de Heyning P. 2007. Validation of the Dutch and the French version of the Tinnitus Questionnaire. *B-ENT* 3 Suppl 7:11–17.
- Melcher JR, Sigalovsky IS, Guinan JJ, Jr., Levine RA. 2000. Lateralized tinnitus studied with functional magnetic resonance imaging: abnormal inferior colliculus activation. *J Neurophysiol* 83:1058–1072.
- Moisset X, Bouhassira D. 2007. Brain imaging of neuropathic pain. *Neuroimage* 37 Suppl 1:S80–S88.
- Moller AR. 1997. Similarities between chronic pain and tinnitus. *Am J Otol* 18:577–585.
- Moller AR. 2000. Similarities between severe tinnitus and chronic pain. *J Am Acad Audiol* 11:115–124.
- Moller AR. 2007. Tinnitus and pain. *Prog Brain Res* 166:47–53.
- Muhlneckel W, Elbert T, Taub E, Flor H. 1998. Reorganization of auditory cortex in tinnitus. *Proc Natl Acad Sci U S A* 95:10340–10343.
- Mulert C, Jager L, Schmitt R, Bussfeld P, Pogarell O, Moller HJ, Juckel G, Hegerl U. 2004. Integration of fMRI and simultaneous EEG: towards a comprehensive understanding of localization and time-course of brain activity in target detection. *Neuroimage* 22:83–94.
- Myles PS, Troedel S, Boquest M, Reeves M. 1999. The pain visual analog scale: is it linear or nonlinear? *Anesth Analg* 89:1517–1520.
- Nichols TE, Holmes AP. 2002. Nonparametric permutation tests for functional neuroimaging: a primer with examples. *Hum Brain Mapp* 15:1–25.
- Pascual-Marqui RD. 2002. Standardized low-resolution brain electromagnetic tomography (sLORETA): technical details. *Methods Find Exp Clin Pharmacol* 24 Suppl D:5–12.
- Pascual-Marqui R. 2007a. Discrete, 3D distributed, linear imaging methods of electric neuronal activity. Part 1: exact, zero error localization. Available from <http://arxiv.org/ftp/arxiv/papers/0710/0710.3341.pdf>
- Pascual-Marqui R. 2007b. Instantaneous and lagged measurements of linear and nonlinear dependence between groups of multivariate time series: frequency decomposition. Available from <http://arxiv.org/abs/0711.1455>.
- Pascual-Marqui RD, Lehmann D, Koukkou M, Kochi K, Anderer P, Saletu B, Tanaka H, Hirata K, John ER, Prichep L, Biscay-Lirio R, Kinoshita T. 2011. Assessing interactions in the brain with exact low-resolution electromagnetic tomography. *Philos Transact A Math Phys Eng Sci* 369:3768–3784.
- Pizzagalli D, Pascual-Marqui RD, Nitschke JB, Oakes TR, Larson CL, Abercrombie HC, Schaefer SM, Koger JV, Benca RM, Davidson RJ. 2001. Anterior cingulate activity as a predictor of degree of treatment response in major depression: evidence from brain electrical tomography analysis. *Am J Psychiatry* 158:405–415.
- Pizzagalli DA, Oakes TR, Fox AS, Chung MK, Larson CL, Abercrombie HC, Schaefer SM, Benca RM, Davidson RJ. 2004. Functional but not structural subgenual prefrontal cortex abnormalities in melancholia. *Mol Psychiatry* 9:325, 393–405.
- Rauschecker JP, leaver AM, Muhlau M. 2010. Tuning out the noise: limbic-auditory interactions in tinnitus. *Neuron* 66:819–826.
- Ribary U, Ioannides AA, Singh KD, Hasson R, Bolton JP, Lado F, Mogilner A, Llinas R. 1991. Magnetic field tomography of coherent thalamocortical 40-Hz oscillations in humans. *Proc Natl Acad Sci U S A* 88:11037–11041.
- Schecklmann M, Landgrebe M, Poepl TB, Kreuzer P, Manner P, Marienhagen J, Wack DS, Kleinjung T, Hajak G, Langguth B. 2013a. Neural correlates of tinnitus duration and distress: a positron emission tomography study. *Hum Brain Mapp* 34:233–240.
- Schecklmann M, Lehner A, Poepl TB, Kreuzer PM, Rupperecht R, Rackl J, Burger J, Frank E, Hajak G, Langguth B, Landgrebe M. 2013b. Auditory cortex is implicated in tinnitus distress: a voxel-based morphometry study. *Brain Struct Funct* 218:1061–1070.
- Schlee W, Hartmann T, Langguth B, Weisz N. 2009. Abnormal resting-state cortical coupling in chronic tinnitus. *BMC Neurosci* 10:11.

- Schlee W, Weisz N, Bertrand O, Hartmann T, Elbert T. 2008. Using auditory steady state responses to outline the functional connectivity in the tinnitus brain. *PLoS One* 3:e3720.
- Schreiber BE, Agrup C, Haskard DO, Luxon LM. 2010. Sudden sensorineural hearing loss. *Lancet* 375:1203–1211.
- Scott B, Lindberg P. 2000. Psychological profile and somatic complaints between help-seeking and non-help-seeking tinnitus subjects. *Psychosomatics* 41:347–352.
- Segrave RA, Cooper NR, Thomson RH, Croft RJ, Sheppard DM, Fitzgerald PB. 2011. Individualized alpha activity and frontal asymmetry in major depression. *Clin EEG Neurosci* 42:45–52.
- Smith SM, Miller KL, Moeller S, Xu J, Auerbach EJ, Woolrich MW, Beckmann CF, Jenkinson M, Andersson J, Glasser MF, Van Essen DC, Feinberg DA, Yacoub ES, Ugurbil K. 2012. Temporally-independent functional modes of spontaneous brain activity. *Proc Natl Acad Sci U S A* 109:3131–3136.
- Smits M, Kovacs S, de Ridder D, Peeters RR, van Hecke P, Sunaert S. 2007. Lateralization of functional magnetic resonance imaging (fMRI) activation in the auditory pathway of patients with lateralized tinnitus. *Neuroradiology* 49:669–679.
- Sullivan MD, Katon W, Dobie R, Sakai C, Russo J, Harrop-Griffiths J. 1988. Disabling tinnitus. Association with affective disorder. *Gen Hosp Psychiatry* 10:285–291.
- Svensson E. 2000. Concordance between ratings using different scales for the same variable. *Stat Med* 19:3483–3496.
- van der Loo E, Congedo M, Vanneste S, De Heyning PV, De Ridder D. 2011. Insular lateralization in tinnitus distress. *Auton Neurosci* 165:191–194.
- van der Loo E, Gais S, Congedo M, Vanneste S, Plazier M, Menovsky T, Van de Heyning P, De Ridder D. (2009a). Tinnitus intensity dependent gamma oscillations of the contralateral auditory cortex. *PLoS One* 4:e7396.
- van Marle HJ, Hermans EJ, Qin S, Fernandez G. 2010. Enhanced resting-state connectivity of amygdala in the immediate aftermath of acute psychological stress. *Neuroimage* 53:348–354.
- Vanneste S, Congedo M, De Ridder D. 2014. Pinpointing a highly specific pathological functional connection that turns phantom sound into distress. *Cereb Cortex* 24:2268–2282.
- Vanneste S, De Ridder D. 2011. Bifrontal transcranial direct current stimulation modulates tinnitus intensity and tinnitus-distress-related brain activity. *Eur J Neurosci* 34:605–614.
- Vanneste S, De Ridder D. 2012a. The Use of Alcohol as a Moderator for Tinnitus-Related Distress. *Brain Topogr* 25:97–105.
- Vanneste S, De Ridder D. 2012b. The auditory and non-auditory brain areas involved in tinnitus. An emergent property of multiple parallel overlapping subnetworks. *Front Syst Neurosci* 6:31.
- Vanneste S, De Ridder D. 2013. Brain areas controlling heart rate variability in tinnitus and tinnitus-related distress. *PLoS One* 8:e59728.
- Vanneste S, Plazier M, der Loo E, de Heyning PV, Congedo M, De Ridder D. 2010a. The neural correlates of tinnitus-related distress. *Neuroimage* 52:470–480.
- Vanneste S, Plazier M, van der Loo E, Ost J, Meeus O, Van de Heyning P, De Ridder D. 2011a. Validation of the Mini-TQ in a Dutch-speaking population. A rapid assessment for tinnitus-related distress. *B-ENT* 7:31–36.
- Vanneste S, Plazier M, van der Loo E, Van de Heyning P, De Ridder D. (2011b). The difference between uni- and bilateral auditory phantom percept. *Clin Neurophysiol* 122:578–587.
- Vanneste S, Plazier M, van der Loo E, Van de Heyning P, De Ridder D. (2010b). The differences in brain activity between narrow band noise and pure tone tinnitus. *PLoS One* 5:e13618.
- Vanneste S, Plazier M, van der Loo E, Ost J, Meeus O, Van de Heyning P, De Ridder D. 2011. Validation of the Mini-TQ in a Dutch-speaking population: a rapid assessment for tinnitus-related distress. *B-ENT* 7:31–36.
- Vanneste S, van de Heyning P, De Ridder D. 2011c. The neural network of phantom sound changes over time: a comparison between recent-onset and chronic tinnitus patients. *Eur J Neurosci* 34:718–731.
- Varela F, Lachaux JP, Rodriguez E, Martinerie J. 2001. The brainweb: phase synchronization and large-scale integration. *Nat Rev Neurosci* 2:229–239.
- Vitacco D, Brandeis D, Pascual-Marqui R, Martin E. 2002. Correspondence of event-related potential tomography and functional magnetic resonance imaging during language processing. *Hum Brain Mapp* 17:4–12.
- Volpe U, Mucci A, Bucci P, Merlotti E, Galderisi S, Maj M. 2007. The cortical generators of P3a and P3b: a LORETA study. *Brain Res Bull* 73:220–230.
- von Leupoldt A, Sommer T, Kegat S, Baumann HJ, Klose H, Dahme B, Buchel C. 2009. Dyspnea and pain share emotion-related brain network. *Neuroimage* 48:200–206.
- von Stein A, Sarnthein J. 2000. Different frequencies for different scales of cortical integration: from local gamma to long range alpha/theta synchronization. *Int J Psychophysiol* 38:301–313.
- Weisz N, Moratti S, Meinzer M, Dohrmann K, Elbert T. 2005. Tinnitus perception and distress is related to abnormal spontaneous brain activity as measured by magnetoencephalography. *PLoS Med* 2:e153.
- Weisz N, Muller S, Schlee W, Dohrmann K, Hartmann T, Elbert T. 2007. The neural code of auditory phantom perception. *J Neurosci* 27:1479–1484.
- Worrell GA, Lagerlund TD, Sharbrough FW, Brinkmann BH, Busacker NE, Cicora KM, O'Brien TJ. 2000. Localization of the epileptic focus by low-resolution electromagnetic tomography in patients with a lesion demonstrated by MRI. *Brain Topogr* 12:273–282.
- Zaehle T, Jancke L, Meyer M. 2007. Electrical brain imaging evidences left auditory cortex involvement in speech and non-speech discrimination based on temporal features. *Behav Brain Funct* 3:63.
- Zumsteg D, Lozano AM, Wennberg RA. 2006a. Depth electrode recorded cerebral responses with deep brain stimulation of the anterior thalamus for epilepsy. *Clin Neurophysiol* 117:1602–1609.
- Zumsteg D, Lozano AM, Wennberg RA. 2006b. Mesial temporal inhibition in a patient with deep brain stimulation of the anterior thalamus for epilepsy. *Epilepsia* 47:1958–1962.
- Zumsteg D, Lozano AM, Wieser HG, Wennberg RA. 2006c. Cortical activation with deep brain stimulation of the anterior thalamus for epilepsy. *Clin Neurophysiol* 117:192–207.
- Zumsteg D, Wennberg RA, Treyer V, Buck A, Wieser HG. 2005. H2(15)O or 13NH3 PET and electromagnetic tomography (LORETA) during partial status epilepticus. *Neurology* 65:1657–1660.

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